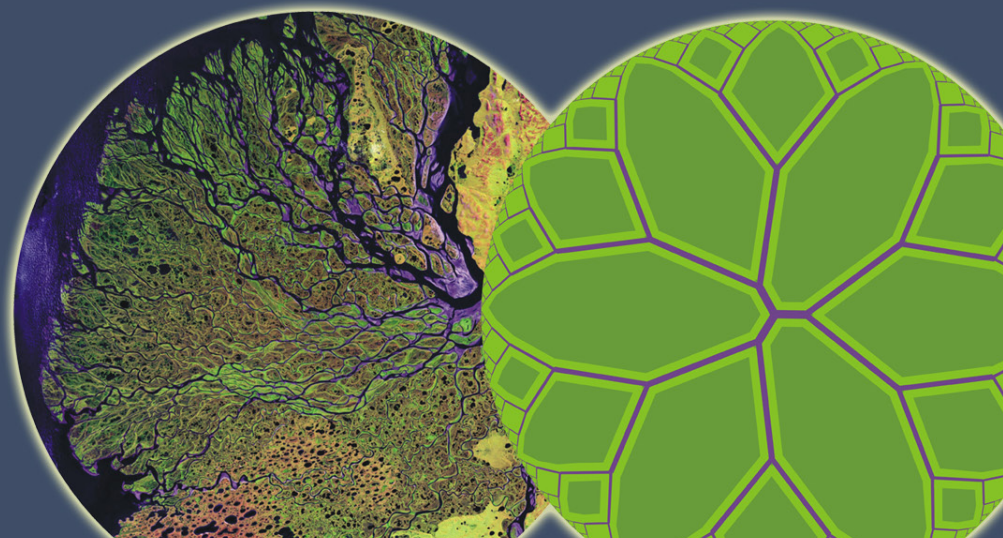


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IS IT HESS-MURRAY LAW ALWAYS VALID?

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Abstract

Complex flow systems such as the vascular and respiratory trees are made of large and small ducts in series. While the literature has reported extensively cases that are in agreement with Hess-Murray law, there are also branching patterns of natural systems that deviate from this law. Is it this deviation to Hess-Murray law possible to predict? In this study, a numerical analysis was carried out to investigate laminar fluid flow of Newtonian and non-Newtonian fluids in T-shaped flow structures with different ratios between the sizes of parent and daughter ducts. The performance of the branching systems was evaluated in terms of total hydraulic resistance and distribution of shear stresses. We showed that the optimal design of a bifurcating ducts not always match a constant reduction factor of $2^{-1/3}$ for the duct sizes. The results were compared with analytical results obtained based on constructal law.

Keywords: tree flow networks, optimal design, Newtonian and non-Newtonian fluids, Hess-Murray law, power-law fluids, numerical study, constructal law.

1. Introduction

Tree-shaped flow networks have been the subject of numerous investigations owing to its importance in understanding the behaviour of natural systems, and for the design of manmade systems [1-4]. Blood vessels supply cellular tissues with

cells, nutrients and oxygen, and remove waste products of cellular activity, through branching vascular networks [5]. The respiratory tree supplies oxygen necessary for tissue metabolism and removes the produced carbon dioxide [6]. Tissues, which make up the respiratory zone of this tree, support a very large gas exchange surface between air and blood that is ventilated and perfused with blood. For a fluid transport system the best flow configuration, that connects a point-to-volume or volume-to-point are tree-shaped, and a compromise must be found between large and small ducts [1-3,7]. For the vascular system, assuming a Hagen–Poiseuille flow through the vessels, Hess [8] and Murray [9] state that the volumetric flow rate must be proportional to the cube of the diameter in a duct optimized to require the minimum work to drive and maintain the fluid. Therefore, the optimal branching is achieved when the cube of the diameter of a parent vessel equals the sum of the cubes of the diameters of the daughters. For symmetric vessels, the ratio between diameters of daughters and parent vessels is $2^{-1/3}$ (Hess-Murray law). This optimum way to connect large and small vessels together having rigid and impermeable walls is only valid as long as the flow is laminar, Newtonian, steady, incompressible and fully developed [5,6,10]. Hess-Murray law has also been shown to describe diverse range of biological networks such as capillaries and many small arteries and veins, airways of conducting zone of the respiratory tract, leaf veins of plants, etc.. Larger arteries and veins, and airways of respiratory zone of the lungs, among others, seem do not follow this $2^{-1/3}$ rule. Besides, turbulent flows would not also be expected to obey to law. In fact, Uylings [11] and Bejan et al. [12] showed that turbulent flows require an optimally $2^{-3/7}$ rule. However, fluid flow in living organisms is essentially laminar and evidences suggest that the exposure to turbulent flows might pose some health risk [6].

Blood includes erythrocytes (red blood cells), leukocytes (white blood cells) and thrombocytes (platelets) in an aqueous solution (plasma). Its rheology is largely influenced by the behaviour of the erythrocytes, mainly due to high concentration [5,13]. Blood flow may be considered as steady or pulsatile, Newtonian or non-Newtonian. In small vessels distant from the heart, the flow may be approached as steady. In larger vessels, the flow is pulsatile due to pumping characteristics induced by the heart. Experimental studies suggest that if vessels experiences high shear rates (higher than 100 s^{-1}), it is reasonable to consider blood flow as a Newtonian fluid [5,13]. However, non-Newtonian effects show up at smaller shear rates in vessels such as the capillaries, small arteries and veins. At shear rates lower than 100 s^{-1} , blood displays shear-thinning behaviour since its viscosity decreases with increasing shear rate. Revellin et al. [14] and Miguel [5] incorporate in their studies non-Newtonian rheology to achieve the optimum way to connect large and small vessels together.

Fåhræus and Lindqvist [15] observed a significant decrease of apparent blood viscosity in tubes with diameters in the range of $50 - 500 \text{ }\mu\text{m}$ (Fåhræus-Lindqvist effect). The reason behind this effect is the formation of a cell-free layer near the wall of the tube, which has a reduced local viscosity (the core of the tube has a higher local viscosity). Blood vessels exhibit diameters from $3 \text{ }\mu\text{m}$ to 3 cm , and studies considering this effect on bifurcating design would be needed. Miguel [13] investigated how the optimal branching of parent to daughter vessels is affected by occurrence of Fåhræus-Lindqvist effect.

Although first derived from the principle of minimum work, Hess-Murray law can be obtained in the light of the constructal law [1-3]. This law is grounded on the idea that flow systems are not purposeless (the ultimate target is to persist) and are free to morph in time (evolve), under global constraints. Shape (structure) is the constructal path to carry fluid, heat, mass, etc., to accomplish their purpose. The constructal laws of vessel's arrangements were derived based on the demand for easier movement, to achieve greater flow access through the generation of a particular design (configuration). Bejan et al. [12] showed that the way to connect large and small vessels together requires a ratio between diameters of daughters and parent vessels of $2^{-1/3}$ (Hess-Murray law) and $2^{-3/7}$ for laminar and turbulent flows, respectively. These authors also derived expressions for the branching angles of vessels that facilitate flow access. Relying on the constructal law, and on analytical approaches, the rules of design for flows of non-Newtonian fluids through bifurcating vessels, and for porous-walled vessels were also predicted [5,6]. These rules for connecting large to small vessels together also depend on fluid behaviour index and on wall permeability. Despite its ubiquity in nature, Hess-Murray's law as a $2^{-1/3}$ rule only maximizes access for Newtonian fluids under laminar flows. Notice that, the rules of design obtained based both on principle of minimum work and on constructal law are based on 1D and 2D analytical approaches. These studies involve many assumptions and simplifications, which are based on justifiable and approximations, listed in [10]. This study aims to obtain new insights into the dynamics of Newtonian and non-Newtonian flows in bifurcating vessels. A 3D numerical study is performed to illustrate fluid flow through T-shaped flow structures. Besides providing a possibility for testing design parameters over a large range of values, the numerical modelling also offers detailed information about the way that the fluid and solid structure interaction occurs. We combine the constructal approach with numerical simulation to analyse these features and to capture the differences between flows profiles in different T-structures. Here, we chart these differences, with the ultimate aim of explaining the features inherent to an easy access to fluid flow.

2. Mathematical Formulation

2.1. Constructal law of design and extremum principles of entropy production

It becomes apparent that the emergence of configuration, defined by the constructal law, requires that the entropy changes, rather than staying the same [1-3,16]. Consider that the fluid flow raised to the power of n is proportional to the pressure difference. The rate of entropy generated, S_g , is

$$\frac{dS_g}{dt} = \frac{Q^n \Delta p}{T} \quad (1)$$

Here Δp is the pressure difference (i.e, the potential), Q is the fluid flow (i.e., the current), and T is the absolute temperature. For a Newtonian fluid $n=1$, the flow is proportional to the pressure difference. In terms of flow resistance R , Eq. 1 may be rewritten as

$$\frac{dS_g}{dt} = \frac{\Delta p^2}{RT} \quad \text{or} \quad R = \frac{\Delta p^2}{(dS_g/dt)T} \quad (2)$$

$$\frac{dS_g}{dt} = \frac{RQ^{2n}}{T} \quad \text{or} \quad R = \frac{T(dS_g/dt)}{Q^{2n}} \quad (3)$$

Maximum flow access means minimum resistance under constraints: constraint of constant Δp or constraint of constant Q . According to the Eq. 2, minimizing the flow resistance for a specified potential (pressure difference), Δp , corresponds to maximization of the entropy generation rate. On the other hand, minimizing the flow resistance under a constant current (fluid flow), Q , corresponds to minimizing the entropy generation rate (Eq. 3).

2.2. Problem description

Here we consider a T-shaped flow system composed by symmetrical cylindrical ducts. Parent duct bifurcate and its size changes by a certain factor according to

$$\frac{D_2}{D_1} = a_D \quad \text{and} \quad \frac{L_2}{L_1} = a_L \quad (4)$$

where D is the diameter, L is the length, and the subscripts 1 and 2 mean parent and daughter tubes. Here we consider geometries with a_D and a_L factors between 0.1 to 1.0. The following geometric constraints are taken into account [12]

$$\frac{\pi}{4} [D_1^2 L_1 + 2D_2^2 L_2] = \text{const} \quad (5)$$

$$2L_1 L_2 = \text{const} \quad (6)$$

The meaning of Eqs. 5 and 6 is that the total volume occupied by the tubes and the total space occupied by the planar assembly of tubes are fixed.

2.3. Governing equations

The flow is considered to be laminar, steady and incompressible. This 3D flow is governed by the continuity equation,

$$\nabla \vec{v} = 0 \quad (7)$$

and the momentum equation

$$\rho \vec{v}(\nabla \vec{v}) = -\nabla P + \nabla \vec{\tau} \quad (8)$$

where v is the velocity, ρ is the density, τ is stress and P is the pressure. The power-law model is used, and an extra-stress tensor is considered

$$\tau_{ij} = \mu Z_{ij} \quad (9)$$

Here Z is the rate of deformation tensor, and the viscosity is

$$\mu = k \dot{\gamma}^{n-1} \exp \frac{T_0}{T} \quad (10)$$

where T is the temperature, T_0 is the reference temperature, μ is the viscosity, k is the consistency index, and n is the power-law index. For $n=1$ this equation becomes the constitutive equation of a Newtonian fluid. For $n<1$ the fluid exhibits shear-thinning properties, and for $n>1$ the fluid has shear-thickening properties. The Reynolds number for these power-law fluid flows is defined as [16]

$$Re_{Dn} = \frac{4^{4-3n} \rho \phi^{2-n}}{\pi^{2-n} K D_1^{4-3n} \left(\frac{3n+1}{4n} \right)^n} \quad (11)$$

where Re_{Dn} is the generalized Metzner–Reed Reynolds.

2.4. Numerical procedure

The governing Eqs. 7–9 are solved using a finite volume method and employing the segregated method with implicit formulation. The SIMPLE algorithm with under-relaxation was selected for the pressure–velocity coupling. At the inlet a constant mass flow rate is assumed. At the outlet, outflow boundary conditions are used to model flow exits where the details of the flow velocity and pressure are

not known prior to solution of the flow problem, the outflow boundary condition assumes a zero normal gradient for all flow variables except pressure. On the walls no-slip boundary conditions are applied. For Eq. 8, the convective term is discretized using second-order-upwind scheme in order to obtain sufficiently accurate solutions. In order to obtain a stable and accurate iterative process, the relaxation factors for momentum and pressure were set to 0.70 and 0.30, respectively. The residual values of the governing Eqs. 7 and 8 were all set to 10^{-4} and 10^{-6} , respectively.

3. Results and discussion

In this section we present a comprehensive set of results to a wider range of power-law indices (i.e., $n=0.776$, $n=1.000$ and $n=1.100$). The generalized Metzner–Reed Reynolds obtained based on Eq. 11 is 100 (i.e., laminar flow). The numerical study was carried out using the following fluids

- Newtonian ($n=1$): $\rho = 1.1405 \text{ kg/m}^3$, $\mu = 1.9043 \times 10^{-5} \text{ Pa.s}$ (air)
 $\rho = 998 \text{ kg/m}^3$, $\mu = 8.91 \times 10^{-4} \text{ Pa.s}$ (water)
 $\rho = 1259.9 \text{ kg/m}^3$, $\mu = 7.99 \times 10^{-1} \text{ Pa.s}$ (glycerin)
- non-Newtonian: shear-thinning ($n=0.776$) $\rho = 1060 \text{ kg/m}^3$;
 $k = 1.47 \times 10^{-4} \text{ Pa.s}^n$ (blood); shear-thickening ($n=1.100$) $\rho = 1260 \text{ kg/m}^3$; $k = 6.60 \times 10^{-3} \text{ Pa.s}^n$.

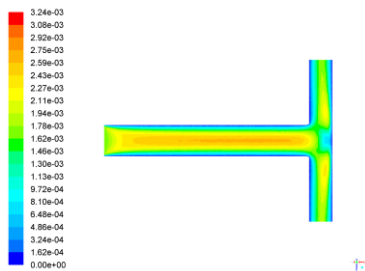


Figure 1.1 Velocity contours (middle plane) for air ($\rho = 1.1405 \text{ kg/m}^3$; $\mu = 1.9043 \times 10^{-5} \text{ Pa.s}$) across a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

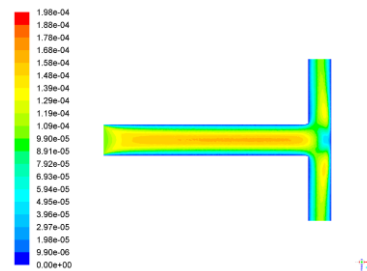


Figure 1.2 Velocity contours (middle plane) water ($\rho = 998 \text{ kg/m}^3$; $\mu = 8.91 \times 10^{-4} \text{ Pa.s}$) across a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

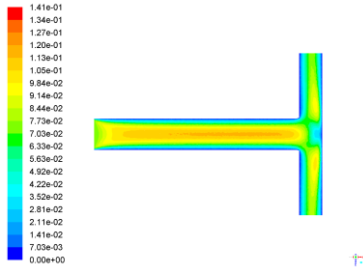


Figure 1.3 Velocity contours (middle plane) glycerin ($\rho = 1259.9 \text{ kg/m}^3$; $\mu = 7.99 \times 10^{-1} \text{ Pa.s}$) across a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

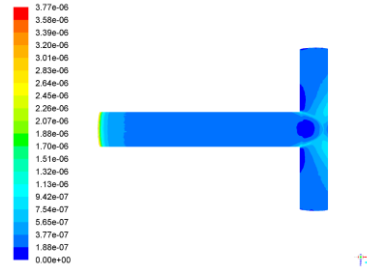


Figure 2.1 Shear stress contours (top plane) for air ($\rho = 1.1405 \text{ kg/m}^3$; $\mu = 1.9043 \times 10^{-5} \text{ Pa.s}$) in a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

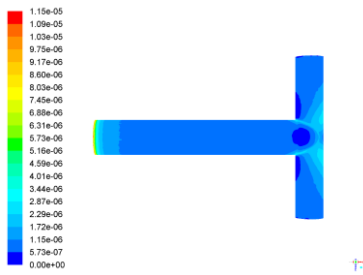


Figure 2.2 Shear stress contours (top plane) water ($\rho = 998 \text{ kg/m}^3$; $\mu = 8.91 \times 10^{-4} \text{ Pa.s}$) in a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

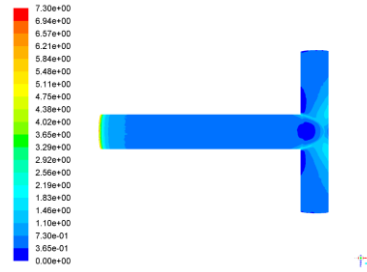


Figure 2.3 Shear stress contours (top plane) glycerin ($\rho = 1259.9 \text{ kg/m}^3$; $\mu = 7.99 \times 10^{-1} \text{ Pa.s}$) in a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

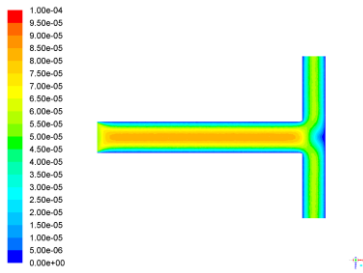


Figure 3 Velocity contours (middle plane) for a shear-thinning fluid ($n=0.776$, $\rho = 1060 \text{ kg/m}^3$; $k = 1.47 \times 10^{-4} \text{ Pa.s}^n$) across a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

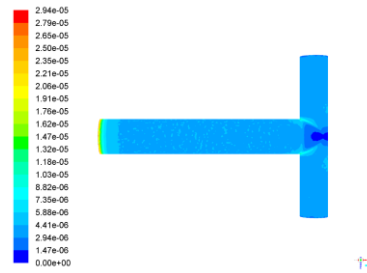


Figure 4 Shear stress contours (top plane) for a shear-thinning fluid ($n=0.776$, $\rho = 1060 \text{ kg/m}^3$; $k = 1.47 \times 10^{-4} \text{ Pa.s}^n$) in a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

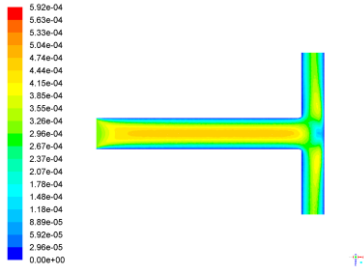


Figure 5 Velocity contours (middle plane) for a shear-thickening fluid ($n=1.100$, $\rho = 1260 \text{ kg/m}^3$; $k = 6.60 \times 10^{-3} \text{ Pa.s}^n$) across a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

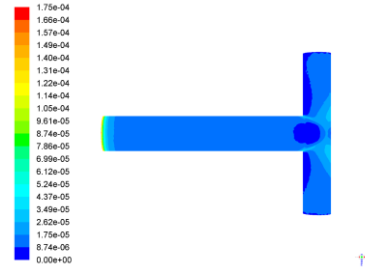


Figure 6 Shear stress contours (top plane) for a shear-thickening fluid ($n=1.100$, $\rho = 1260 \text{ kg/m}^3$; $k = 6.60 \times 10^{-3} \text{ Pa.s}^n$) in a T-shaped flow structure designed according to $D_2/D_1 = L_2/L_1 = 2^{-1/3}$

Figures 1 and 2 show the velocity and shear stress contours for the Newtonian fluids. Although air, water and glycerine have different viscosities and densities, the velocity and the shear stress profiles are similar. We also find that the flow distribution throughout the T-structure is not uniform. This means that for a symmetric bifurcation the flow distribution is asymmetric. This is in agreement with the findings presented in the studies conducted by Andrade Jr et al. [17], and Pepe et al. [10]. The distribution of shearing stress is also significantly heterogeneous in the structure.

Velocity and shear stress contours taken for power law fluids, which include shear thinning and shear thickening, in T-shaped flow geometries are depicted in Figs. 3 to 6. Velocity and shear stress profiles are different for both fluids, and are also different from the profiles observed for Newtonian fluids. In addition, shear thickening fluid flow has in common with Newtonian flows a heterogeneous flow distribution in a symmetric branched assembly of tubes. On the other hand, fluid flow and shear stress distributions are homogeneous for shear thinning flow. It has been found a dependence of flow asymmetric on Reynolds number [10]. Ours study suggest that, for a given Reynolds number, the flow distribution depends on power-law index n .

It would be interesting to study the flow resistance for the T-assembly of ducts. According to Eq. 3, maximum flow access means minimizing the flow resistance under a constant current that corresponds to minimizing the entropy generation rate.

Figure 7 show the total dimensionless flow resistance, R^* , for flows of Newtonian and non-Newtonian flow through T-shaped structures. The dimensionless resistance R^* is defined as form according to

$$R^* = \frac{R}{R_{D=L=2^{-1/3}}} \quad (12)$$

where R is total flow resistance defined as the ratio between the pressure difference and the mass flow rate through the T-structure, and $R_{D=L=2^{-1/3}}$ is the total flow resistance in a T-shaped assembly of ducts designed according to D_2/D_1

$= L_2/L_1 = 2^{-1/3}$. Based on Fig. 7, the geometry that allows the minimum system-resistance is obtained. Table 1 shows these optimal values and the values predicted analytically by Revellin et al. [14] and Miguel [5].

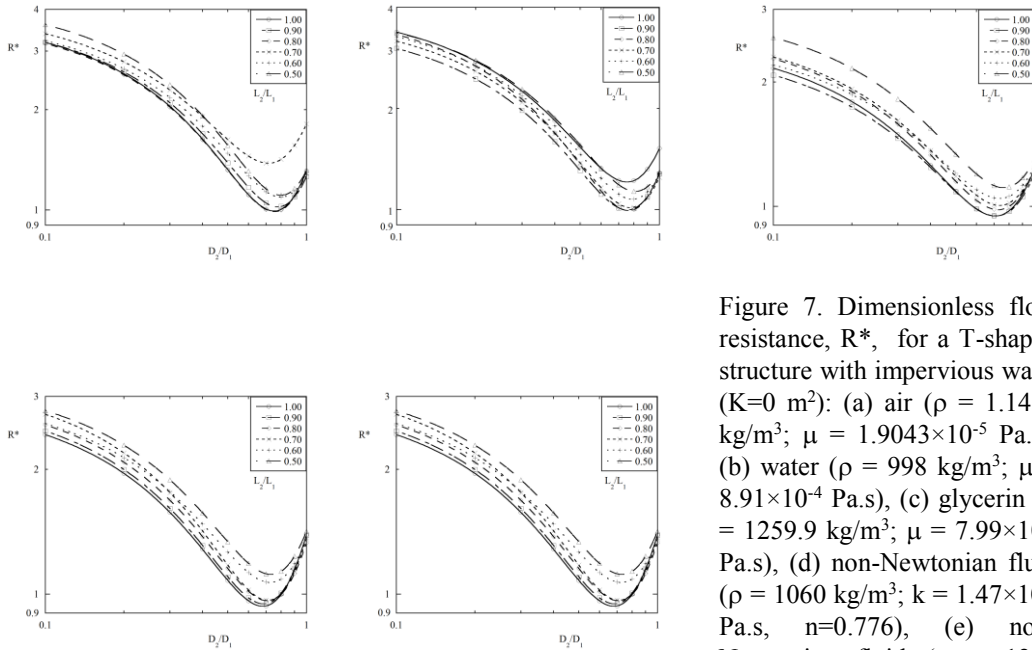


Figure 7. Dimensionless flow resistance, R^* , for a T-shaped structure with impervious walls ($K=0 \text{ m}^2$): (a) air ($\rho = 1.1405 \text{ kg/m}^3$; $\mu = 1.9043 \times 10^{-5} \text{ Pa.s}$), (b) water ($\rho = 998 \text{ kg/m}^3$; $\mu = 8.91 \times 10^{-4} \text{ Pa.s}$), (c) glycerin ($\rho = 1259.9 \text{ kg/m}^3$; $\mu = 7.99 \times 10^{-1} \text{ Pa.s}$), (d) non-Newtonian fluid ($\rho = 1060 \text{ kg/m}^3$; $k = 1.47 \times 10^{-4} \text{ Pa.s}$, $n=0.776$), (e) non-Newtonian fluid ($\rho = 1260 \text{ kg/m}^3$; $k = 6.60 \times 10^{-34} \text{ Pa.s}$, $n=1.1$)

Table 1. Optimal branching sizes for a T-shaped assembly of ducts

power-law index n	Optimal assembly of ducts based on Fig.7		Optimal assembly of ducts based on analytical models of Revellin et al. [14] and Miguel [5]	
	D_2/D_1	L_2/L_1	D_2/D_1	L_2/L_1
0.776	0.71	1.00	0.77	0.84
1.000	0.79	0.79	0.79	0.79
1.100	0.70	1.00	0.80	0.78

According to Table 1, there is a difference between results obtained based on analytical models and on our numerical study. In an attempt to understand these discrepancies, our numerical results are used to estimate the flow resistance in different location of the T-assembly of ducts (Table 2).

Table 2. Flow resistance per length for T-shaped assembly of ducts

Total Flow Resistance (Pa.s ⁿ /kg)	$D_2/D_1 = L_2/L_1 = 0.8$			$D_2/D_1 = 0.7 \quad L_2/L_1 = 1.0$		
	Power-law index n					
	0.776	1.000	1.100	0.776	1.000	1.100
Parent duct	0.0031696	0.0069743	0.0013718	0.0023109	0.0051059	0.0009587
Daughter duct 1	0.0010482	0.0026487	0.0005035	0.0015061	0.0036656	0.0006791
Daughter duct 2	0.0010499	0.0026613	0.0005065	0.0015034	0.0037740	0.0006932
Connection parent-daughter ducts	0.0003489	0.0014065	0.0002629	0.0004579	0.0015127	0.0002694
Total	0.0045675	0.0110359	0.0021397	0.0042735	0.0103379	0.0019141

Notice that, analytical approaches developed by Revellin et al. [14] and Miguel [5] consider that the losses on the connection of large and small vessels together are negligible compared with friction losses through the vessels. Besides, they also assume a homogeneous flow distribution occurring in symmetric branched structures. According to Table 2, it is remarkable to notice that, the resistance in each daughter duct is not the same. This is a direct consequence of heterogeneous flow distribution in the branched structure. Besides, the flow resistance at the connection between parent and daughter ducts is not negligible as compared to the resistances of parent and daughter tubes. Higher resistance occurs for Newtonian fluids, and lower resistances for shear-thickening fluids. Although, they are of the same order of magnitude, the total resistance of T-assembly of $D_2/D_1 = 0.7$ and $L_2/L_1 = 1.0$ ducts is slightly lower than the T-assembly of $D_2/D_1 = L_2/L_1 = 0.8$ ducts but the resistance of daughter ducts is higher. This is an interesting result and deserves a further analysis.

To explain these results, it is quite intuitive to consider the fluid flow like the flow of electric charges (electric current). For any system (fluid or electric charges), the total flowrate must be the same (principle of continuity). In our flow system, parent duct and the duct that connects parent-daughter ducts are resistors connected in series, and the daughter ducts are resistors connected in parallel. The total equivalent resistance of the resistors is

$$R_t \sim R_p + R_c + \frac{R_{d1} R_{d2}}{R_{d1} + R_{d2}} \quad (13)$$

where R is the resistance and the subscripts t, p, c, d1 and d2 mean total equivalent, parent duct, connection parent-daughter ducts, d1 daughter duct 1 and d2 daughter duct 2, respectively. Eq. 13 reproduces rather well the numerical values depicted in Table 2. Notice that R_{d1} and R_{d2} are much lower than 1 Pa.sⁿ/kg. Examination values depicted in Table 1 and Eq. 13, suggests that the resistance of daughter ducts play a critical role on total equivalent resistance. A small increase of the resistance of daughter ducts causes a decrease of the total

equivalent resistance of the flow system.

4. Conclusions

From the findings presented in this study, the following main conclusions can be drawn

- i) The flow is strongly dependent on the power-law index.
- ii) Asymmetric flow occurs in symmetric T-branched structures.
- iii) Different flow resistances occur in each daughter duct.
- iv) Losses on the connection of large and small vessels together are not negligible.
- v) Optimal branching sizes for T-shaped assemblies of ducts obtained in this numerical study do not agree completely with the results obtained with analytical models.

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